

Cerebral Autoregulation in Carotid Artery Occlusive Disease Assessed From Spontaneous Blood Pressure Fluctuations by the Correlation Coefficient Index

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Background and Purpose—Estimation of dynamic cerebral autoregulation from spontaneous fluctuations of arterial blood pressure (ABP) and cerebral blood flow velocity (CBFV) is an attractive monitoring option for cerebral hemodynamic impairment. We evaluated the correlation coefficient index method in patients with severe obstructive carotid disease and compared it with transfer function analysis (frequency domain approach to cerebral autoregulation) and CO₂ vasomotor reactivity.

Methods—In 139 patients with severe unilateral carotid stenosis ($\geq 70\%$) or occlusion, CBFV (transcranial Doppler) and ABP (Finapres method) were recorded over 10 minutes. Correlations between systolic pressure, diastolic pressure, and mean ABP and CBFV oscillations over 1-minute epochs were averaged over 10 minutes to form the correlation coefficient indexes (Sx, Dx, Mx, respectively). Transfer function parameters (phase shift and gain between ABP and CBFV oscillations) were determined from the entire 10-minute period. CO₂ reactivity was assessed by inhalation of 7% CO₂.

Results—The correlation indexes Dx and Mx were significantly higher ipsilateral to stenosis and increased with degree of stenosis, indicating increasing dependence of CBFV on ABP and thus impairment of cerebral autoregulation. Dx and Mx correlated moderately but highly significantly with transfer function parameters and CO₂ reactivity and showed a good level of agreement in detecting pathological values. Patients with a small variance of the 1-minute source correlations of Dx and Mx showed clearly better correlation values. Transfer function parameters and CO₂ reactivity but not Dx and Mx were significantly poorer in patients with symptomatic stenosis or occlusion.

Conclusions—The potential of the correlation coefficient indexes Dx and Mx in detecting hemodynamic impairment in patients with carotid stenosis is comparable to that of transfer function analysis and CO₂ reactivity testing. In future, a combination of various hemodynamic tests might help to identify patients at risk for ischemic events.

Key Words: autoregulation ■ carbon dioxide ■ carotid stenosis

Cerebrovascular pressure autoregulation is a protective intrinsic control mechanism of the cerebral circulation that keeps cerebral blood flow independent from systemic changes in blood pressure.¹ In clinical states associated with chronic hemodynamic compromise such as obstructive carotid artery disease, detection of impaired cerebral autoregulation might help to identify patients at risk from stroke as shown for cerebrovascular reserve capacity.^{2,3}

Clinical assessment of cerebral autoregulation is based on various concepts. Over many years, the upper and lower arterial blood pressure (ABP) limits of autoregulatory maintenance of cerebral blood flow were assessed, requiring considerable manipulation of ABP. Over the last decade, the high temporal resolution of transcranial Doppler sonography

allowed analysis of the amplitude and time latencies of the cerebral blood flow velocity (CBFV) response to rapid but relatively small changes in ABP (dynamic cerebral autoregulation).⁴ Reliable and repeatable noninvasive induction of ABP changes, however, proved difficult. Over the last years, attention has therefore been directed toward analyzing physiologically occurring ABP changes without the need for any external manipulation.

Two main approaches to analyzing dynamic cerebral autoregulation from such spontaneous ABP fluctuations have been used so far. The first one works in the frequency domain. Via transfer function analysis, the phase shift and gain between spontaneous (or respiratory-induced) oscillations of ABP and CBFV are calculated.⁵ Mainly, a positive

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TABLE 1. Results of Various Cerebral Autoregulatory Parameters and CO₂ Reactivity in Different Groups of Stenosis

	Degree of Stenosis				Significances, Ipsi- vs Contralateral	Intergroup
	A, 70–79% (N=40), Unilateral	B, 80–89% (n=21), Unilateral	C, 90–99% (N=56), Unilateral	D, 100% (n=22), Unilateral		
Correlation coefficient indices						
Sx ipsilateral	0.28±0.18	0.34±0.16	0.33±0.19	0.32±0.25	A,B†, C*	NS
Sx contralateral	0.21±0.21	0.26±0.13	0.22±0.19	0.29±0.21		NS
Dx ipsilateral	0.08±0.16	0.15±0.14	0.25±0.19	0.26±0.24	A,B,C‡, D†	A-C‡, A-D†
Dx contralateral	0.01±0.15	0.00±0.15	0.01±0.13	0.11±0.22		NS
Mx ipsilateral	0.35±0.18	0.45±0.11	0.51±0.18	0.51±0.21	A,B,C‡, D†	A-C‡, A-D†
Mx contralateral	0.27±0.17	0.28±0.11	0.30±0.17	0.39±0.17		NS
Transfer function analysis						
LF phase ipsilateral (°)	38.8±22.2	34.9±24.5	20.4±24.5	19.0±25.8	A,B†, C,D‡	A-C‡, A-D†
LF phase contralateral	44.8±20.8	55.9±25.5	44.8±27.9	39.6±20.5		
HF gain ipsilateral (cm/s) · mm Hg ⁻¹	0.75±0.27	0.63±0.26	0.59±0.28	0.49±0.28	A,C‡, B,D†	A-D‡, A-C†
HF gain contralateral	0.97±0.34	0.97±0.47	1.03±0.34	0.87±0.35		
CO ₂ -reactivity						
Ipsilateral (cm/s) · mm Hg ⁻¹	1.92±0.78	1.32±0.86	1.06±0.70	1.17±1.09	A,B†, C,D‡	A-C‡, A-B†, A-D†
Contralateral	2.16±0.78	1.97±0.73	1.95±0.66	2.34±0.80		

**P*<0.05; †*P*<0.01; ‡*P*<0.001

phase shift between ABP and CBFV oscillations (ie, CBFV oscillations precede ABP oscillations) was interpreted as intact cerebral autoregulation according to a high-pass filter model of the cerebral autoregulatory feedback control system.^{6,7} Both transfer function phase and gain were found to be reduced in patients with carotid artery stenosis.^{6,8,9}

The second approach works in the time domain. Its rationale is based on the classic assumption of independence of cerebral blood flow from a wide range of ABP or cerebral perfusion pressure (autoregulatory plateau). Thus, quite simply, a correlation index of ≈0 indicates functioning autoregulation, whereas a correlation index of ≈1 denotes impaired autoregulation. This method has been largely validated in sedated patients suffering from traumatic brain injury, correlating well with static cerebral autoregulation and clinical outcome.^{10–12} Little is known so far, however, of its applicability to other, nonsedated patient groups. Furthermore, the correlation coefficient index method has never been compared with the transfer function analysis approach or, in a larger series, with the conventional assessment of CO₂ reserve capacity.

This study aims (1) to evaluate the correlation coefficient index method in patients with severe carotid artery stenosis or occlusion and (2) to compare this approach with results from transfer function analysis and CO₂ reactivity testing.

Patients and Methods

We studied 150 patients (mean age, 67±8 years; 18 women) with severe unilateral stenosis (≥70%) or occlusion of the internal carotid artery (ICA). Exclusion criteria included an insufficient temporal bone window, relevant stenosis of the middle cerebral artery (MCA), current atrial fibrillation, and >4 ventricular extra beats per minute. Grading of stenosis was performed by use of Doppler velocities combined with B-mode imaging.¹³ Medium-grade, hemodynam-

ically insignificant contralateral stenosis (50% to 69%) was present in 29 patients. Patients considered for final analysis were assigned to different groups on the basis of degree of ipsilateral ICA stenosis (Table 1). Carotid stenosis or occlusion was defined as clinically symptomatic if hemispheric or retinal ischemic symptoms (transient ischemic attack or stroke) ipsilateral to the affected side had occurred during the previous 2 years.

Measurements were performed with subjects in a supine position with 45° inclination of the upper body. CBFV was measured in both MCAs by insonation through the temporal bone window with 2-MHz transducers (Multidop-X4, DWL). Continuous noninvasive ABP recording was achieved via a servocontrolled finger plethysmograph (Finapres 2300, Ohmeda) with the subject's right hand positioned at heart level. End-tidal CO₂ partial pressure (PETCO₂) was measured with an infrared capnometer (Normocap, Datex) during nasal expiration. After stable baseline values had been established, a data segment of 10 minutes was recorded with the patient breathing spontaneously. ABP, heart rate, and PETCO₂ levels, determined at the beginning and end of this period, did not show substantial differences between the different groups. CO₂ reactivity was assessed via inhalation of room air mixed with 7% CO₂.

All parameters were recorded online at a sampling rate of 100 Hz and further analyzed with custom-written software developed in house. The mean length of analyzed time series of spontaneous oscillations of ABP and CBFV was 565±65 seconds.

Correlation Coefficient Analysis

This analysis was done according to several investigations (M.C. and colleagues) that showed that fluctuations on a long time scale in CBFV are more or less correlated with fluctuations in ABP.^{12,14} To quantify the degree of correlation, Pearson's correlation coefficient was used. In the first step, mean, systolic, and diastolic values of ABP and CBFV were averaged over 3-second periods. Then, 20 consecutive 3-second averages of mean, systolic, and diastolic ABP and CBFV were used to calculate single Pearson's correlation coefficients (ie, for every 1-minute period; see Figure 1). Finally, the collected 1-minute systolic, diastolic, and mean correlation coefficients were averaged over the whole measurement period and labeled as the autoregulatory indexes Mx, Sx, and Dx, respectively. These 3 indexes thus mirror the averaged grade of correlation of systolic,

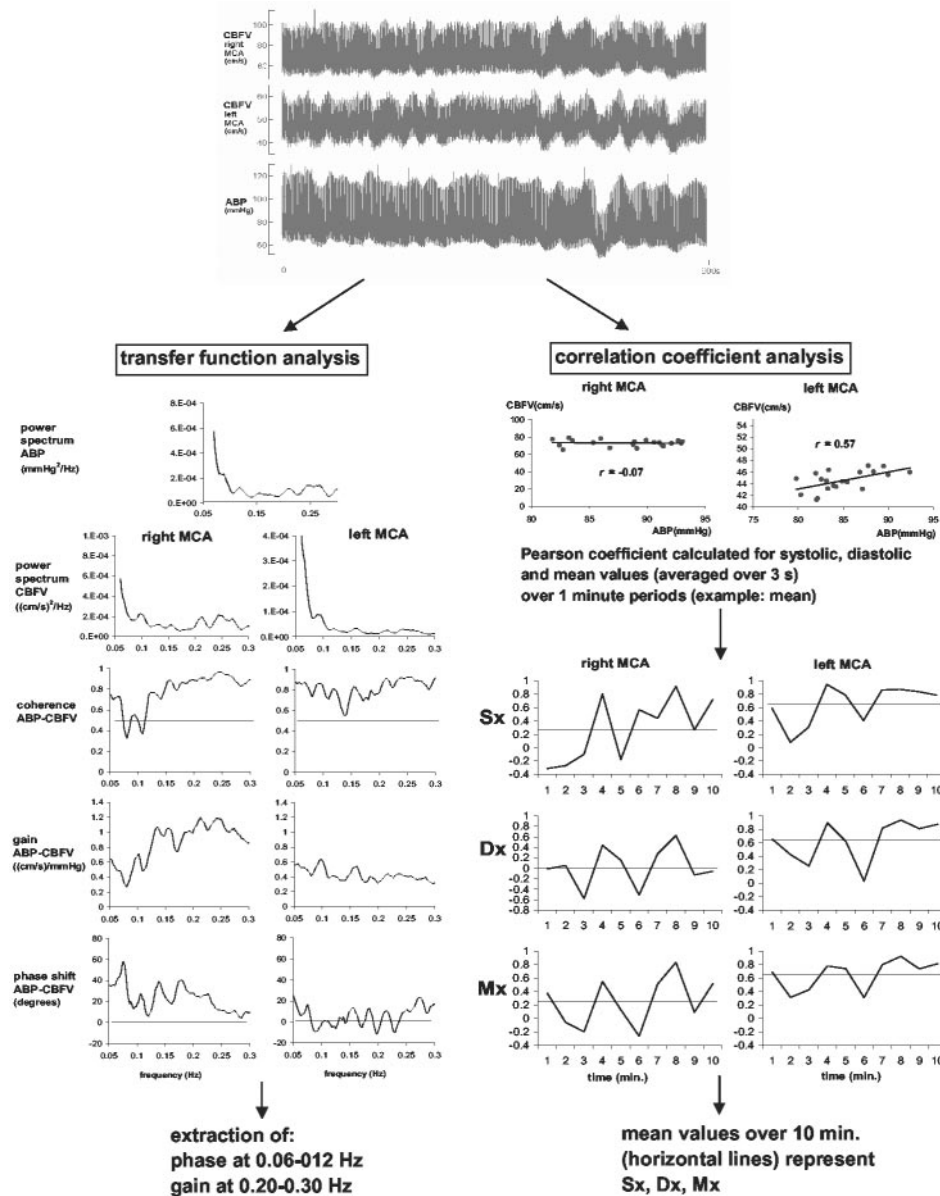


Figure 1. A 59-year-old woman with occlusion of the left ICA. Transfer function analysis: A frequency of ≈ 0.065 Hz was selected for phase extraction on both sides. Phase shift was clearly reduced on the affected left side. Gain was analyzed at 0.25 Hz. Note the lacking high-pass filter properties of the gain spectrum over the affected side, leading to a clear side-to-side difference at this frequency. Correlation coefficient analysis: In the upper tracings, an example of a 1-minute period is shown. Note the dependency of CBFV on ABP over the affected left side (positive Pearson coefficient). Average of 10 correlation coefficients over 10 minutes was calculated as Sx, Dx, and Mx. Note the consistently higher mean value (horizontal lines) on the affected side, but also the variability of the single correlation coefficients over the analyzed 10-minute period.

diastolic, and mean ABP and CBFV fluctuations. For data sets not ending with a whole 1-minute period (eg, total eligible length of 9.8 minutes), the last period was also allowed for calculation if it was >0.5 minutes.

Various prefiltering of the data for reduction of spectral noise (>0.05 Hz, >0.15 Hz), other lengths of the primary data segments (5 or 10 seconds instead of 3 seconds), and the use of a moving window for calculation of the correlation coefficients did not yield better results in terms of intergroup differences and variances. For reasons of simplicity, we therefore present results of data analyzed without prefiltering and moving window calculation.

Transfer Function Analysis

We have described this method in detail elsewhere.^{15,16} In short, the periodograms and cross-periodogram of ABP and CBFV were

computed by discrete Fourier transform, and the auto-spectra and cross-spectrum were estimated by smoothing the respective periodograms with a triangular window.¹⁶ The coherence spectrum is defined as the normalized modulus of the cross-spectrum; the phase spectrum is the argument of the (complex-valued) cross-spectrum. Finally, the gain is essentially the regression coefficient of CBFV on ABP.

The coherence at any frequency is a number between 0 and 1, where 0 indicates no linear relationship and 1 indicates perfect linear dependence of the signals at the given frequency. With the smoothing we used, the coherence is significant (at the 95% level) if it is >0.49 . If the coherence is not significantly different from 0, the phase spectrum cannot be used for analysis, because under the hypothesis of zero coherence, the phase spectrum is uniformly distributed over the interval $[-\pi, \pi]$.¹⁷ For estimation of the cerebral

autoregulatory capacity, a low-frequency range (LF, 0.06 to 0.12 Hz) and a high-frequency range (HF, 0.20 to 0.30 Hz) were analyzed. The applied rules for phase extraction are described elsewhere.^{15,18} Briefly, an area within the target frequency range that showed a maximum coherence of CBFV and ABP oscillations for both MCA sides and was not affected by discontinuities in the estimated phase spectrum was selected. We concentrated on the phase shift between ABP and CBFV oscillations in the LF range and the gain between ABP and CBFV oscillations in the HF range. These were the most meaningful parameters in previous studies.^{8,15}

We included 139 patients in the final analysis. We excluded 11 data sets because of a lack of significant coherence of spontaneous oscillations in the LF band.

Assessment of CO₂ Reactivity

This assessment was done by dividing the maximum percentage increase of CBFV during hypercapnia (averaged over 1 respiratory cycle) by the absolute increase in PETCO₂ (in mm Hg).

Statistical Analysis

Statistical analysis of intraindividual and interindividual differences and correlations was carried out with nonparametric tests (Kruskal-Wallis, Wilcoxon, Spearman's rank coefficient). We used the closed test principle to control the multiple significance level taken in the case of multiple testing for differences among the 4 groups. A value of $P < 0.05$ was considered statistically significant. Data are reported as mean \pm SD.

For calculating the level of agreement (LA) between methods of detection of pathological values, cutoff values for the pathological range of affected sides were defined as poorer than the 10% quantile of the unaffected sides (Mx, ≥ 0.51 ; Dx, > 0.22 ; LF phase, $\leq 18^\circ$; HF gain, ≤ 0.61 (cm/s) \cdot mm Hg⁻¹; CO₂ reactivity, $\leq 1.24\%$ /mm Hg). Then, the LA for affected sides was calculated as the portion of those patients classified identically by both methods.

Results

Figure 1 illustrates raw data and application of autoregulation analysis.

Correlation Coefficient Autoregulatory Indexes Mx, Sx, and Dx in Different Groups of Stenosis

A clear side-to-side difference was found in unilateral stenosis $\geq 80\%$ for the autoregulatory indexes Dx and Mx but not for Sx (Table 1 and Figure 2). In addition, in terms of intergroup differences, the autoregulatory indexes Mx and Dx proved to be more useful than Sx. For Mx, differentiation between different degrees of stenosis was most pronounced between groups A and B; groups C and D tended to have poorer values. A similar trend was observed for the autoregulatory index Dx.

Comparison of the Correlation Coefficient Autoregulatory Indexes With Autoregulatory Indexes Derived From Transfer Function Analysis and CO₂ Reactivity

Moderate but highly significant correlations were found between autoregulatory indexes Dx and Mx and the phase shift and gain of transfer function analysis. Significant correlations were also found when Dx and Mx were compared with conventional CO₂ vasomotor reactivity (Table 2 and Figure 3). Between-group differences and within-group variances of the autoregulatory indexes Dx and Mx were generally comparable with those of conventional CO₂ reactivity (Figure 2). The LA in detection of pathological values with transfer function parameters was moderate to good (Dx

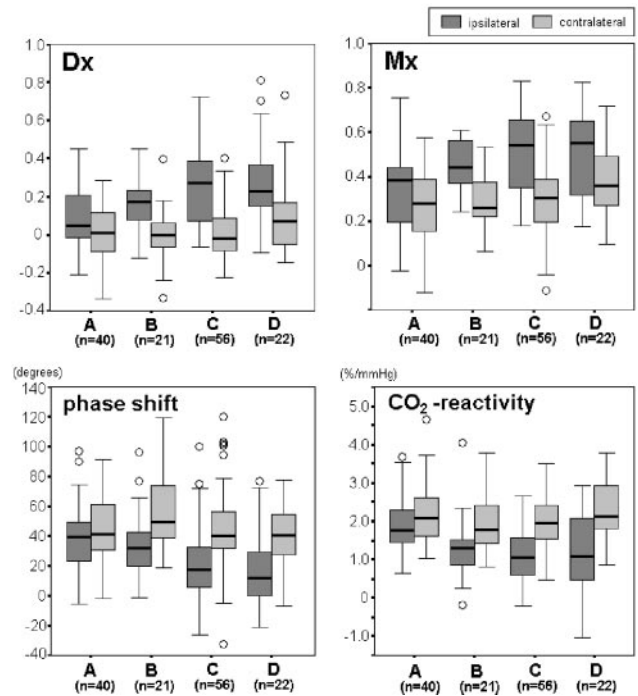


Figure 2. Box plots of autoregulation parameters in different groups of ICA stenosis. \circ , Denotes exceeding values (> 1.5 box length). Significances and definition of groups A through D are given in Table 1.

with phase/gain, 0.61/0.64; Mx with phase/gain, 0.60/0.63). The LA between Dx/Mx and CO₂ reactivity was 0.69/0.68. For comparison, the LA between phase/gain and CO₂ reactivity was 0.66/0.51. No significant correlation between any cerebral autoregulatory parameter and average PETCO₂ during the spontaneous breathing period was found.

Methodological Aspects of Calculating the Correlation Coefficient Indexes

The absolute standard deviations of the subsequent source correlation values (SCSD) averaged for calculation of the respective autoregulatory indexes Sx, Mx, and Dx were slightly smaller over affected sides (significant only for Mx, $P < 0.001$). There was a slight but highly significant trend toward lower SCSD for Dx and Mx compared with Sx ($P < 0.001$). A significant inverse correlation between SCSD and the respective autoregulatory indexes Sx and Mx but not Dx was found (r , up to -0.52 ; $P < 0.001$). Analysis of the correlation coefficient indexes from the lowest and highest quartile of SCSD separately shows clearly better correlations with transfer function parameters and CO₂ reactivity for the lowest quartile of SCSD (Table 2).

To assess the influence of various lengths of measurement periods on Mx and Dx, values calculated from data segments shorter than the full 10-minute period were correlated with those from the full period. It turned out that Mx and Dx values calculated from data segments up from a duration of 4 minutes showed a high and stable correlation ($r > 0.84$) with values calculated from the full period.

Relation to Clinical Status

The mean degree of stenosis was only slightly higher in symptomatic patients ($90 \pm 8\%$ versus $86 \pm 9\%$, $P = 0.014$).

TABLE 2. Results of Correlation Analysis

All Sides (n=278) Quartiles (n=70)	Versus LF		Versus HF		Versus CO ₂	
	phase <i>r</i>	<i>P</i>	gain <i>r</i>	<i>P</i>	Reactivity <i>r</i>	<i>P</i>
Sx, all sides	-0.37	<0.001	-0.09	NS	-0.24	<0.001
Sx, low-quartile SCSD	-0.31	0.009	0.01	NS	-0.26	0.027
Sx, high-quartile SCSD	-0.35	0.003	0.04	NS	0.10	NS
Dx, all sides	-0.40	<0.001	-0.33	<0.001	-0.38	<0.001
Dx, low-quartile SCSD	-0.47	<0.001	-0.52	<0.001	-0.45	<0.001
Dx, high-quartile SCSD	-0.25	0.036	-0.14	NS	-0.34	0.005
Mx, all sides	-0.39	<0.001	-0.30	<0.001	-0.34	<0.001
Mx, low-quartile SCSD	-0.59	<0.001	-0.46	<0.001	-0.49	<0.001
Mx, high-quartile SCSD	-0.13	NS	-0.33	0.006	-0.13	NS
LF phase					0.39	<0.001
HF gain					0.25	<0.001

The correlation coefficient autoregulatory parameters showed no significant difference between clinically symptomatic and asymptomatic patients, whereas transfer function parameters and CO₂ reactivity differed significantly between these 2 groups (Figure 4). Analyzing the quartile of patients with the lowest SCSD did not result in significant improvement in differentiation between asymptomatic and symptomatic patients for the correlation coefficient index method.

Discussion

Best treatment strategies for patients with severe ICA stenosis or occlusion are under debate. Large trials have shown that there is only a small overall benefit of carotid endarterectomy in patients with asymptomatic stenosis, whereas extra-intracranial bypass surgery for carotid occlusion was of no benefit even in symptomatic patients.^{19,20} However, the fact that association of severe carotid stenosis or occlusion with chronic cerebral hemodynamic compromise bears a considerably increased risk of stroke has become more evident over the last years.^{2,3,21} Therefore, routine characterization of the cerebral hemodynamic status might become increasingly important in the therapeutic management of patients with carotid stenosis or occlusion by identifying those patients at highest risk of stroke. In the present study, we showed that estimating the cerebral autoregulatory capacity from spontaneous fluctuations in ABP is an attractive, completely noninvasive option for assessing intrinsic cerebral hemodynamics.

Methodological Aspects

The correlation coefficient index method has evolved as a method for continuous, noninvasive monitoring of cerebral autoregulation over the last decade.^{11,12} The main methodological problem of the correlation coefficient index approach in our series was the strong variation of the 1-minute source correlation coefficients (Figure 1). Already in previous studies analyzing long-term recordings over hours in head-injured patients, a considerable variation of the source correlation coefficients could be observed.¹² In these investigations, at least 30-minute averaging of Mx has been recommended to filter out random fluctuations of ABP and CBFV. We found that with a data assessment length of 4 minutes, the absolute Mx and Dx values did not relevantly differ from the 10-minute period. The length of data assessment might therefore not be the only relevant factor. The extent of variation in the 1-minute source correlations (SCSD) substantially influenced absolute correlation coefficient index values and correlation with other methods. Thus, the SCSD might reflect the extent of signal noise and random fluctuations of ABP and CBFV as a critical parameter for calculation of the correlation coefficient indexes.

In contrast to previous studies applying the correlation coefficient index method in head-injured patients, the autoregulatory index Dx appeared to be more useful than Sx in our patients. This can be explained by the possible disturbance of diastolic cerebral blood flow resulting from a high intracranial pressure in brain-injury patients, rendering the autoregulatory index Dx unreliable.

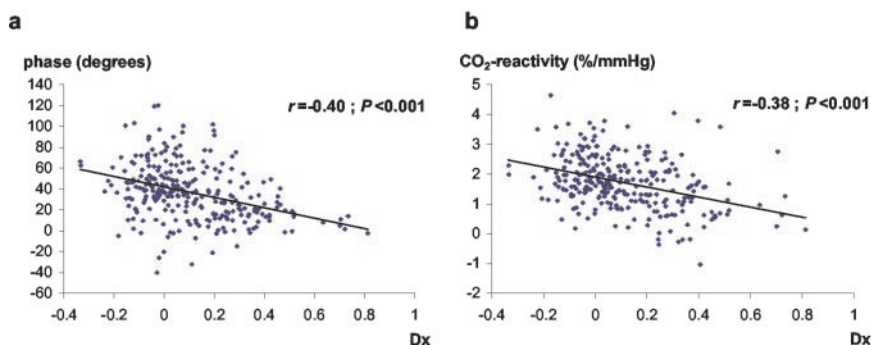


Figure 3. Illustrative scatterplots (n=278 MCA sides). a, Autoregulatory index Dx with phase shift of transfer function; b, Autoregulatory index Dx with CO₂ reactivity.

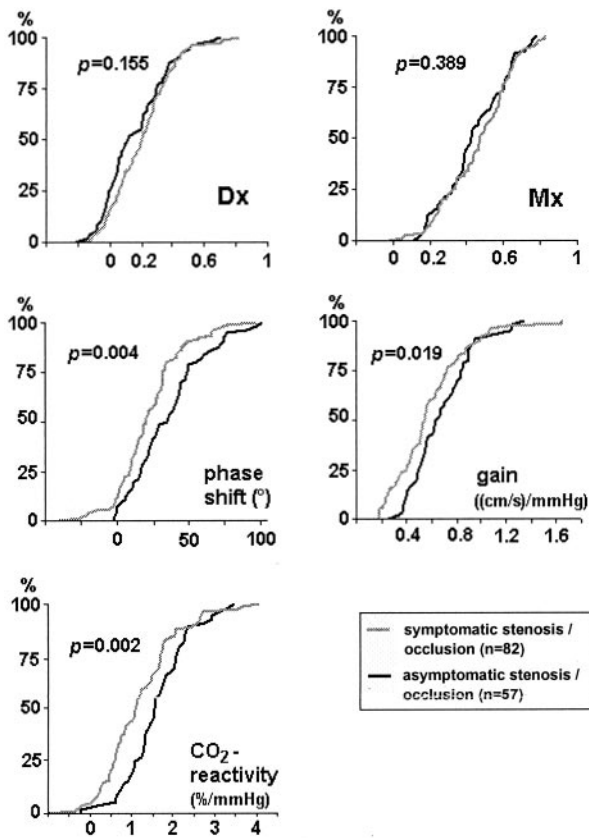


Figure 4. Cumulative distribution of autoregulatory parameters and CO₂ reactivity with regard to the presence or absence of previous clinical symptoms ipsilateral to the affected ICA side (symptomatic vs asymptomatic stenosis). Note that, for Dx and Mx, smaller values indicate better autoregulation, whereas for the remaining parameters, smaller values indicate a poorer state. Probability values indicate significances between symptomatic and asymptomatic patients.

Application to Patients With Obstructive Carotid Disease

The increase in the indexes Mx and Dx with increasing degree of stenosis indicates an increasing dependence of CBFV on ABP and thus impairment of cerebral autoregulation. The lack of difference between preocclusive stenosis and occlusion may be explained by the lacking hemodynamic difference between these 2 states. We also found a considerable overlap among different degrees of stenosis, which was also observed for parameters of transfer function analysis and CO₂ reactivity. This overlap is based on the fact that not only the degree of stenosis but also the quality of intracranial collateral flow compensation determine the extent of hemodynamic compromise.²²

Comparison With Transfer Function Analysis

From a basic physiological point of view, the correlation coefficient indexes might be related to the phase shift calculated from transfer function analysis. Translating the phase shift into the time domain, a phase shift toward 0 means no relevant time delay between slow oscillations of ABP and CBFV. This should result in a higher positive correlation between these signals and thus a higher correlation coefficient

index.^{14,23} Indeed, we found a moderate to good LA in detecting pathological values by both methods and a moderate overall correlation.

The gain of the transfer function between ABP and CBFV oscillations is principally more difficult to interpret. As observed previously, absolute values of transfer function gain were significantly smaller for affected ICA sides, decreasing further with increasing degree of stenosis.^{8,15,24,25} This does not necessarily indicate a more intact autoregulatory damping effect of ABP amplitude changes. It might rather be interpreted as the inability of achieving active autoregulatory diameter changes in (sub)maximally dilated cerebral arterioles, leading to reduced CBFV amplitude oscillations.²⁴ However, the real interpretation of the gain as an autoregulatory parameter remains unresolved, and correlations with other established autoregulatory tests have not yet been performed. However, our study does show a highly significant negative correlation and a good LA in detecting pathological values between the autoregulatory indexes Mx and Dx and transfer function gain, supporting in principle the pathophysiological significance of this parameter. The correlation of gain with CO₂ reactivity was better in a previous study.⁸ Reasons for this difference remain unclear; probably the different HF ranges (0.15 to 0.40 Hz versus 0.20 to 0.30 Hz in our study) might play a role.

Overall, a clear superiority of either transfer function analysis or the correlation coefficient approach regarding correlation and agreement with CO₂ reactivity and side-to-side and intergroup differences could not be found.

Comparison With CO₂ Vasomotor Reactivity

Measuring the cerebrovascular reserve capacity is the most widely established method for assessing cerebral hemodynamic compromise in patients with obstructive carotid disease so far.²¹ It is based on the assumption that reflex vasodilation occurs with reduced poststenotic perfusion pressure and that further vasodilation as a reaction to a stimulus such as CO₂ or acetazolamide is hence reduced. This has been found to be of prognostic relevance with regard to future cerebral ischemic events.^{2,3} Our study confirmed this ability by the significant difference between symptomatic and asymptomatic patients. Absolute correlations between Dx and Mx and CO₂ reactivity were only moderate. On the other hand, we could show a comparatively good LA in detecting pathological values between the autoregulatory indexes Dx and Mx and CO₂ reactivity. Although the cerebral autoregulatory system has a more complex nature by involving intrinsic sensing of blood flow and controlling of cerebral arterioles, a principal pathophysiological relationship between both methods, which do have cerebral arterioles as a common effector organ, might thus exist.

Comparison With Clinical Status

We found that previously symptomatic patients have significantly poorer cerebral autoregulation as calculated from transfer function analysis of spontaneous blood pressure oscillations. This has not been reported yet and supports the probable prognostic value of autoregulatory parameters for cerebral ischemic events. Correlation coefficient parameters,

however, did not differ significantly between symptomatic and asymptomatic stenosis. This might point to a better pathophysiological validity of transfer function analysis and CO₂ reactivity regarding detection of clinically relevant hemodynamic impairment in terms of ischemic events. However, prospective studies will have to evaluate this topic.

Conclusions

The correlation coefficient method as a measure of cerebral autoregulation in chronic obstructive carotid artery disease has a power to detect hemodynamic impairment comparable to that of the conventional CO₂ reactivity test and transfer function analysis. We suggest introducing this approach and transfer function analysis to hemodynamic testing in patients with carotid artery disease.

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References

- Paulson OB, Strandgaard S, Edvinsson L. Cerebral autoregulation. *Cerebrovasc Brain Metab Rev*. 1990;2:161–192.
- Markus H, Cullinane M. Severely impaired cerebrovascular reactivity predicts stroke and TIA risk in patients with carotid artery stenosis and occlusion. *Brain*. 2001;124:457–467.
- Silvestrini M, Vernieri F, Pasqualetti P, Matteis M, Passarelli F, Troisi E, Caltagirone C. Impaired cerebral vasoreactivity and risk of stroke in patients with asymptomatic carotid artery stenosis. *JAMA*. 2000;283:2122–2127.
- Aaslid R, Lindegaard KF, Sorteberg W, Nornes H. Cerebral autoregulation dynamics in humans. *Stroke*. 1989;20:45–52.
- Zhang R, Zuckerman JH, Giller CA, Levine BD. Transfer function analysis of dynamic cerebral autoregulation in humans. *Am J Physiol*. 1998;274:H233–H241.
- Diehl RR, Linden D, Lucke D, Berlitz P. Phase relationship between cerebral blood flow velocity and blood pressure: a clinical test of autoregulation. *Stroke*. 1995;26:1801–1804.
- Diehl RR, Linden D, Lucke D, Berlitz P. Spontaneous blood pressure oscillations and cerebral autoregulation. *Clin Auton Res*. 1998;8:7–12.
- Hu HH, Kuo TB, Wong WJ, Luk YO, Chern CM, Hsu LC, Sheng WY. Transfer function analysis of cerebral hemodynamics in patients with carotid stenosis. *J Cereb Blood Flow Metab*. 1999;19:460–465.
- Lang EW, Diehl RR, Mehdorn HM. Cerebral autoregulation testing after aneurysmal subarachnoid hemorrhage: the phase relationship between arterial blood pressure and cerebral blood flow velocity. *Crit Care Med*. 2001;29:158–163.
- Lang EW, Mehdorn HM, Dorsch NW, Czosnyka M. Continuous monitoring of cerebrovascular autoregulation: a validation study. *J Neurol Neurosurg Psychiatry*. 2002;72:583–586.
- Czosnyka M, Smielewski P, Piechnik S, Pickard JD. Clinical significance of cerebral autoregulation. *Acta Neurochir Suppl (Wien)*. 2002;81:117–119.
- Czosnyka M, Smielewski P, Kirkpatrick P, Menon DK, Pickard JD. Monitoring of cerebral autoregulation in head-injured patients. *Stroke*. 1996;27:1829–1834.
- de Bray JM, Glatt B. Quantification of atheromatous stenosis in the extracranial internal carotid artery. *Cerebrovasc Dis*. 1995;5:414–426.
- Piechnik SK, Yang X, Czosnyka M, Smielewski P, Fletcher SH, Jones AL, Pickard JD. The continuous assessment of cerebrovascular reactivity: a validation of the method in healthy volunteers. *Anesth Analg*. 1999;89:944–949.
- Reinhard M, Müller T, Guschlbauer B, Timmer J, Hetzel A. Transfer function analysis for clinical evaluation of dynamic cerebral autoregulation: a comparison between spontaneous and respiratory-induced oscillations. *Physiol Meas*. 2003;24:27–43.
- Timmer J, Lauk M, Deuschl G. Quantitative analysis of tremor time series. *Electroencephalogr Clin Neurophysiol*. 1996;101:461–468.
- Brockwell PJ, Davis RA. *Time Series: Theory and Methods*. New York, NY: Springer; 1991.
- Kuo TB, Chern CM, Sheng WY, Wong WJ, Hu HH. Frequency domain analysis of cerebral blood flow velocity and its correlation with arterial blood pressure. *J Cereb Blood Flow Metab*. 1998;18:311–318.
- Enderterectomy for asymptomatic carotid artery stenosis: Executive Committee for the Asymptomatic Carotid Atherosclerosis Study. *JAMA*. 1995;273:1421–1428.
- Failure of extracranial-intracranial arterial bypass to reduce the risk of ischemic stroke: results of an international randomized trial: the EC/IC Bypass Study Group. *N Engl J Med*. 1985;313:1191–1200.
- Derdeyn CP, Grubb RL Jr, Powers WJ. Cerebral hemodynamic impairment: methods of measurement and association with stroke risk. *Neurology*. 1999;53:251–259.
- Müller M, Schimrigk K. Vasomotor reactivity and pattern of collateral blood flow in severe occlusive carotid artery disease. *Stroke*. 1996;27:296–299.
- Steinmeier R, Bauhuf C, Hubner U, Bauer RD, Fahlbusch R, Laumer R, Bondar I. Slow rhythmic oscillations of blood pressure, intracranial pressure, microcirculation, and cerebral oxygenation: dynamic interrelation and time course in humans. *Stroke*. 1996;27:2236–2243.
- Diehl RR, Diehl B, Sitzer M, Hennerici M. Spontaneous oscillations in cerebral blood flow velocity in normal humans and in patients with carotid artery disease. *Neurosci Lett*. 1991;127:5–8.
- Bazner H, Daffertshofer M, Konietzko M, Hennerici MG. Modification of low-frequency spontaneous oscillations in blood flow velocity in large- and small-artery disease. *J Neuroimaging*. 1995;5:212–218.